

Echocardiographic Evaluation of Prosthetic Valves

Dr. Myla Gloria Salazar - Supe



The 1st valve replacement in 1960

It will work: The first successful mitral valve replacement ☆

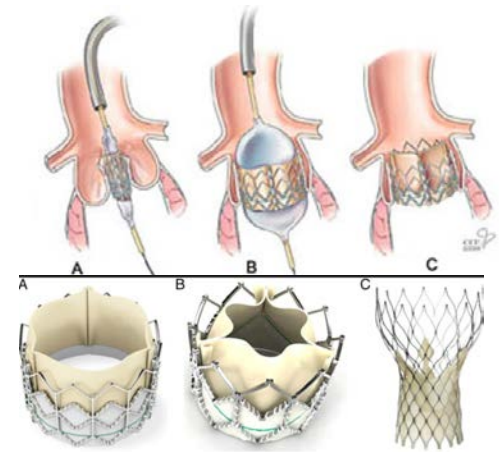
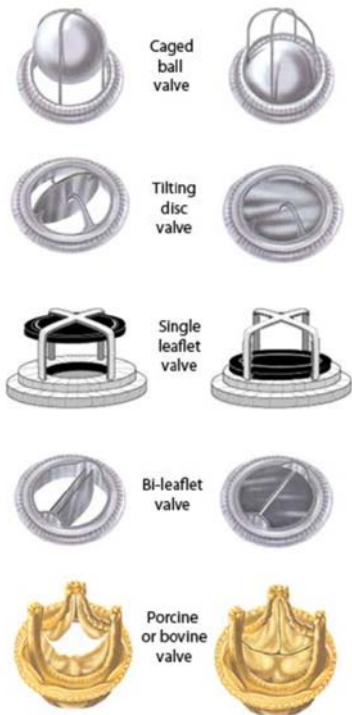
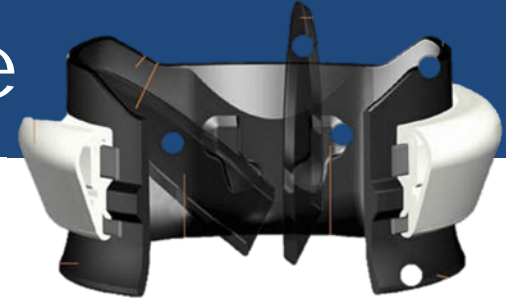
Nina S. Braunwald, MD 🧑

Abstract

In 1959, a prosthetic mitral valve of flexible polyurethane with Teflon chordae tendineae was designed and fabricated. After a series of experiments in dogs carried out at the Clinic of Surgery at the National Heart Institute, on March 11, 1960, this valve was used as a total replacement of the mitral valve of a 44-year-old woman with mitral regurgitation. After an uneventful postoperative course, she was discharged from the hospital and did well thereafter, but died suddenly, presumably of an arrhythmia, 4 months after operation.



There is no perfect valve



“they have introduced other, new problems into clinical medicine, so that in effect, the patient is exchanging one disease process for another”

Basic Principles

- By their design, almost all replacement valves are **obstructive** compared with normal native valves
- Most mechanical valves and many biologic valves are associated with trivial or mild transprosthetic regurgitation (**physiologic regurgitation**)
- Because of **shielding and artifacts**, insonation of the valve esp regurgitant jets may be difficult and requires multiple angulations of the probe and the use of off-axis view

Normal Values for Implanted Aortic Valves

AORTIC VALVES	SIZE (mm)	PEAK GRADIENT (mm Hg)	MEAN GRADIENT (mm Hg)	EFFECTIVE ORIFICE AREA (cm ²)
Carpentier-Edwards Pericardial <i>Stented bovine pericardial</i>	19	32.1 ± 3.4	24.2 ± 8.6	1.2 ± 0.3
	21	25.7 ± 9.9	20.3 ± 9.1	1.5 ± 0.4
	23	21.7 ± 8.6	13.0 ± 5.3	1.8 ± 0.3
	25	16.5 ± 5.4	9.0 ± 2.3	
Carpentier-Edwards Standard <i>Stented porcine</i>	19	43.5 ± 12.7	25.6 ± 8.0	0.9 ± 0.2
	21	27.7 ± 7.6	17.3 ± 6.2	1.5 ± 0.3
	23	28.9 ± 7.5	16.1 ± 6.2	1.7 ± 0.5
	25	24.0 ± 7.1	12.9 ± 4.6	1.9 ± 0.5
	27	22.1 ± 8.2	12.1 ± 5.5	2.3 ± 0.6
	29		9.9 ± 2.9	2.8 ± 0.5
Hancock <i>Stented porcine</i>	21	18.0 ± 6.0	12.0 ± 2.0	
	23	16.0 ± 2.0	11.0 ± 2.0	
	25	15.0 ± 3.0	10.0 ± 3.0	
Hancock II <i>Stented porcine</i>	21		14.8 ± 4.1	1.3 ± 0.4
	23	34.0 ± 13.0	16.6 ± 8.5	1.3 ± 0.4
	25	22.0 ± 5.3	10.8 ± 2.8	1.6 ± 0.4
	29	16.2 ± 1.5	8.2 ± 1.7	1.6 ± 0.2
Medtronic Mosaic <i>Stented porcine</i>	21		14.2 ± 5.0	1.4 ± 0.4
	23	23.8 ± 11.0	13.7 ± 4.8	1.5 ± 0.4
	25	22.5 ± 10.0	11.7 ± 5.1	1.8 ± 0.5
	27		10.4 ± 4.3	1.9 ± 0.1
	29		11.1 ± 4.3	2.1 ± 0.2
Medtronic-Hall <i>Single tilting disc</i>	20	34.4 ± 13.1	17.1 ± 5.3	1.2 ± 0.5
	21	26.9 ± 10.5	14.1 ± 5.9	1.1 ± 0.2
	23	26.9 ± 8.9	13.5 ± 4.8	1.4 ± 0.4
	25	17.1 ± 7.0	9.5 ± 4.3	1.5 ± 0.5
	27	18.9 ± 9.7	8.7 ± 5.6	1.9 ± 0.2
St. Jude Medical Standard <i>Bileaflet</i>	19	42.0 ± 10.0	24.5 ± 5.8	1.5 ± 0.1
	21	25.7 ± 9.5	15.2 ± 5.0	1.4 ± 0.4
	23	21.8 ± 7.5	13.4 ± 5.6	1.6 ± 0.4
	25	18.9 ± 7.3	11.0 ± 5.3	1.9 ± 0.5
	27	13.7 ± 4.2	8.4 ± 3.4	2.5 ± 0.4
	29	13.5 ± 5.8	7.0 ± 1.7	2.8 ± 0.5

Normal Values for Implanted Mitral Valves

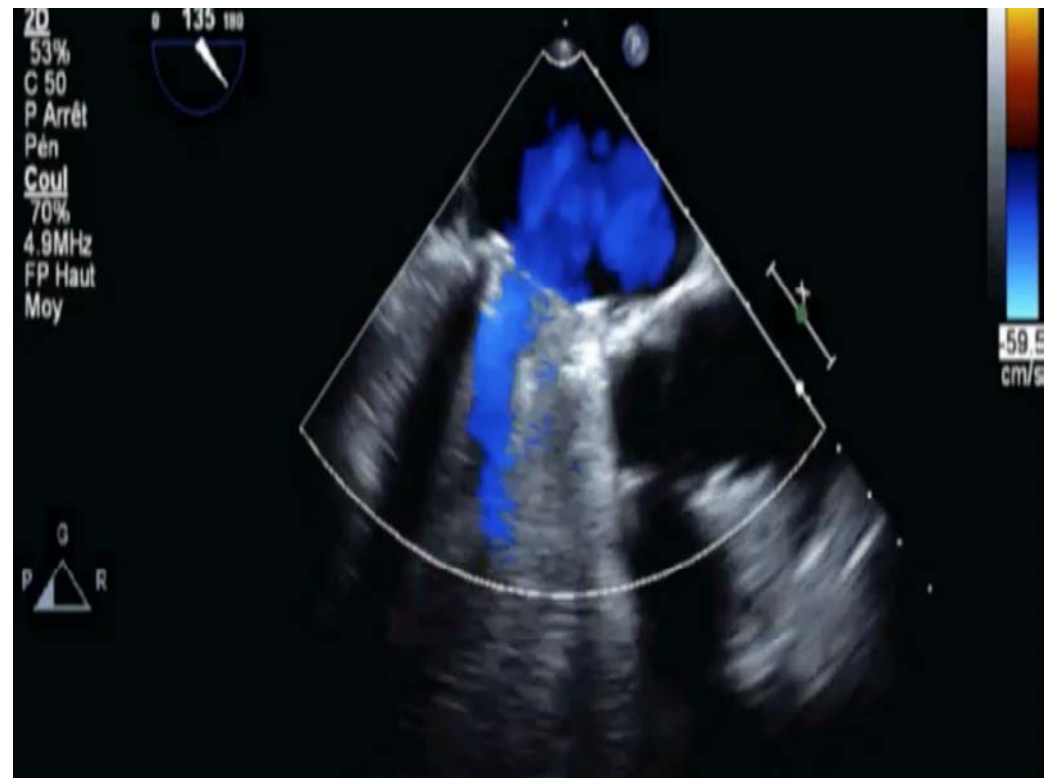
MITRAL VALVES	SIZE (mm)	GRADIENT (mm Hg)	GRADIENT (mm Hg)	PEAK VELOCITY (m/sec)	PRESSURE HALF-TIME (msec)	ORIFICE AREA (cm ²)
Carpentier-Edwards <i>Stented bioprosthesis</i>	27		6 ± 2	1.7 ± 0.3	98 ± 28	
	29		4.7 ± 2	1.76 ± 0.27	92 ± 14	
	31		4.4 ± 2	1.54 ± 0.15	92 ± 19	
	33		6 ± 3		93 ± 12	
Carpentier-Edwards Pericardial <i>Stented bioprosthesis</i>	27		3.6	1.6	100	
	29		5.25 ± 2.36	1.67 ± 0.3	110 ± 15	
	31		4.05 ± 0.83	1.53 ± 0.1	90 ± 11	
	33		1	0.8	80	
Hancock I or not specified <i>Stented bioprosthesis</i>	27	10 ± 4	5 ± 2		115 ± 20	1.3 ± 0.8
	29	7 ± 3	2.46 ± 0.79		95 ± 17	1.5 ± 0.2
	31	4 ± 0.86	4.86 ± 1.69		90 ± 12	1.6 ± 0.2
	33	3 ± 2	3.87 ± 2			1.9 ± 0.2
Hancock II <i>Stented bioprosthesis</i>	27					2.21 ± 0.14
	29					2.77 ± 0.11
	31					2.84 ± 0.1
	33					3.15 ± 0.22
Medtronic-Hall <i>Tilting disc</i>	27			1.4	78	
	29			1.57 ± 0.1	69 ± 15	
	31			1.45 ± 0.12	77 ± 17	
St. Jude Medical <i>Bileaflet</i>	23		4	1.5	160	1
	25		2.5 ± 1	1.34 ± 1.13	75 ± 4	1.35 ± 0.17
	27	11 ± 4	5 ± 1.82	1.61 ± 0.29	75 ± 10	1.67 ± 0.17
	29	10 ± 3	4.15 ± 1.8	1.57 ± 0.29	85 ± 10	1.75 ± 0.24

Basic Principles

- By their design, almost all replacement valves are **obstructive** compared with normal native valves
- Most mechanical valves and many biologic valves are associated with trivial or mild transprosthetic regurgitation (**physiologic regurgitation**)
- Because of **shielding and artifacts**, insonation of the valve esp regurgitant jets may be difficult and requires multiple angulations of the probe and the use of off-axis view

Physiologic Regurgitation

- **Washing jets** to prevent thrombus formation
- 10-15%
- Jets low in momentum
 - homogeneous in color,
 - aliasing mostly confined to the base of the jet.



Basic Principles

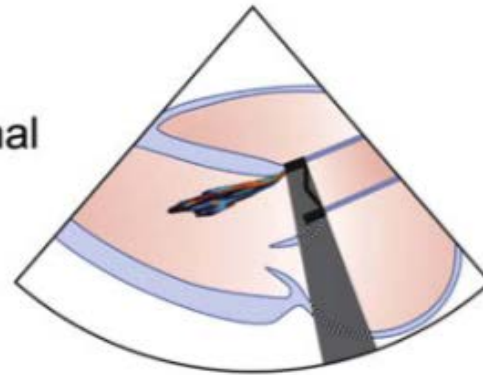
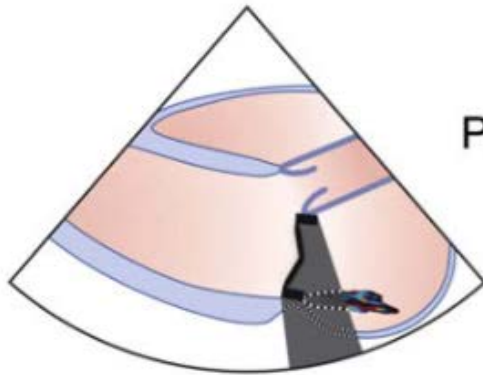
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Shadowing

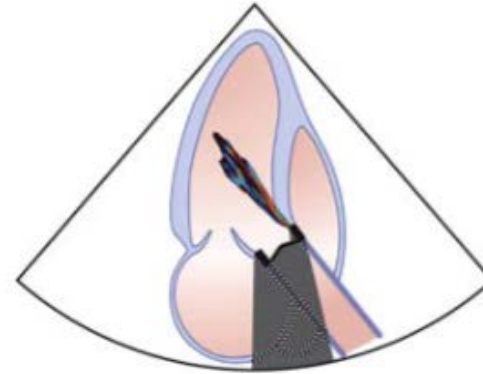
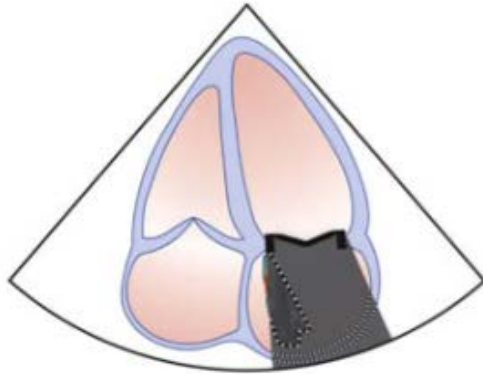
Mitral prosthesis

Aortic prosthesis

Parasternal




Apical



Types of Prosthetic Valves

Table 1 Types of prosthetic heart valves



Biologic

Stented

Porcine xenograft

Pericardial xenograft

Stentless


Porcine xenograft

Pericardial xenograft

Homograft (allograft)

Autograft

Percutaneous

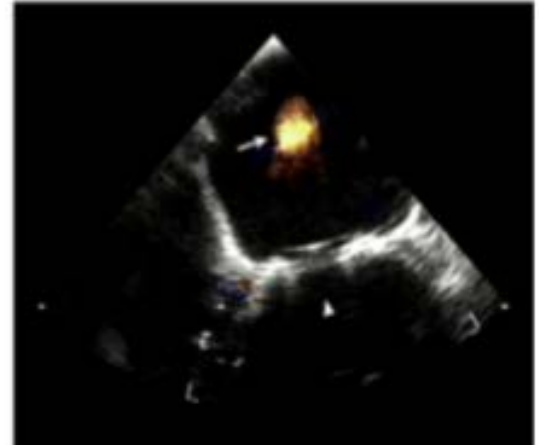
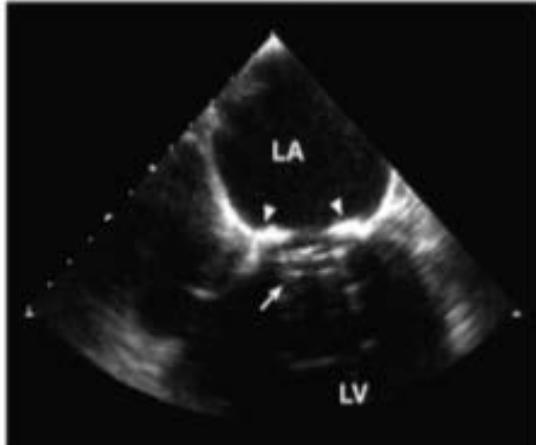
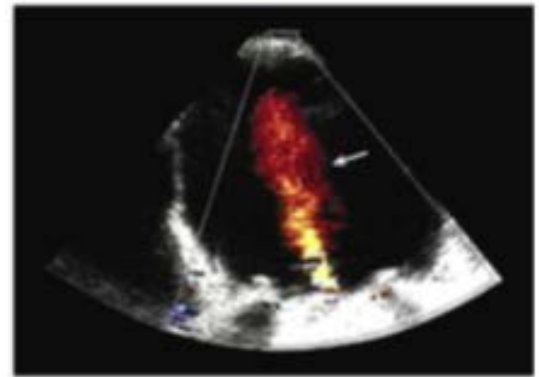
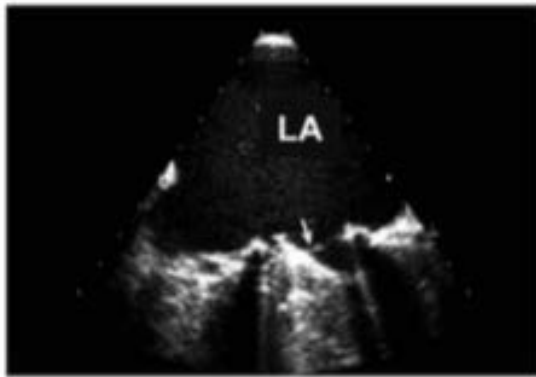
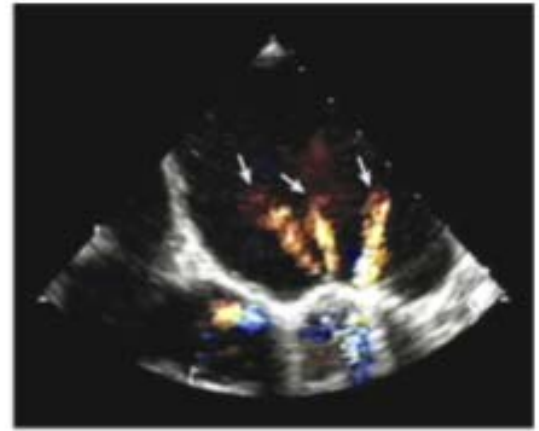
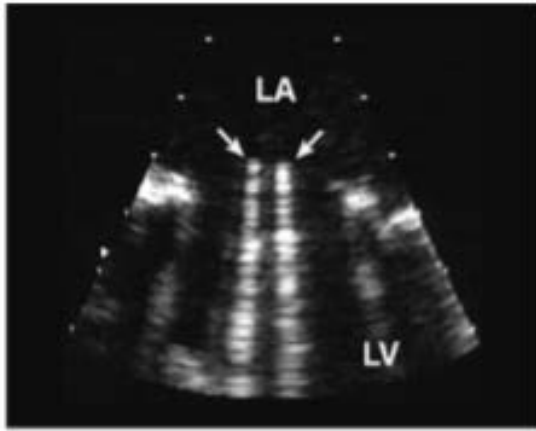


Mechanical

Bileaflet

Single tilting disc

Caged-ball



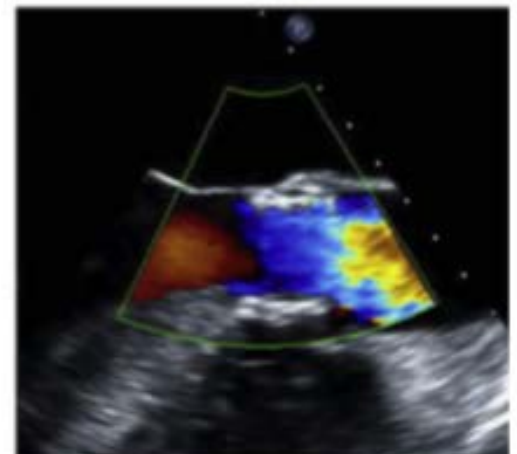
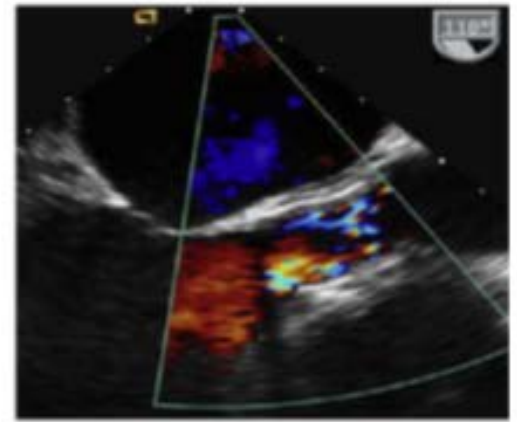
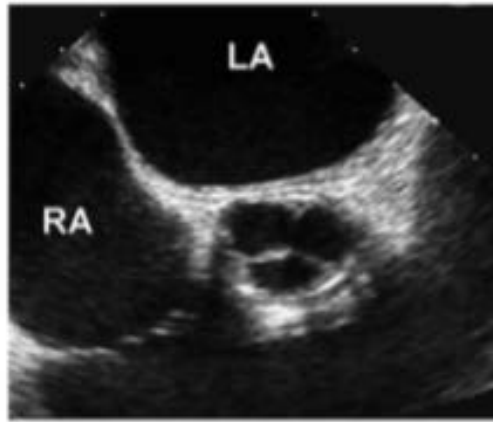
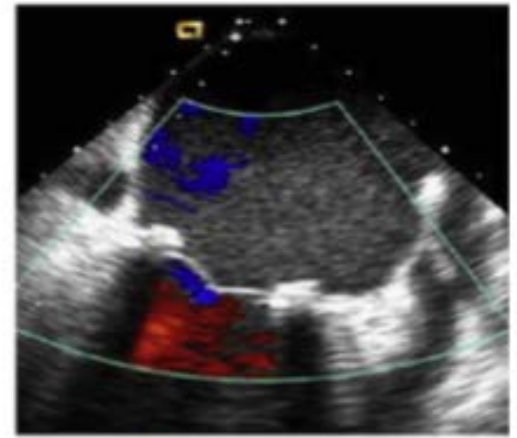


Table 2 Essential parameters in the comprehensive evaluation of prosthetic valve function

	Parameter
Clinical information	Date of valve replacement Type and size of the prosthetic valve Height, weight, body surface area Symptoms and related clinical findings Blood pressure and heart rate
Imaging of the valve	Motion of leaflets or occluder Presence of calcification on the leaflets or abnormal echo densities on the various components of the prosthesis Valve sewing ring integrity and motion
Doppler echocardiography of the valve	Contour of the jet velocity signal Peak velocity and gradient Mean pressure gradient VTI of the jet DVI Pressure half-time in MV and TV. EOA* Presence, location, and severity of regurgitation [†]
Other echocardiographic data	LV and RV size, function, and hypertrophy LA and right atrial size Concomitant valvular disease Estimation of pulmonary artery pressure
Previous postoperative studies, when available	Comparison of above parameters is particularly helpful in suspected prosthetic valvular dysfunction

PVM

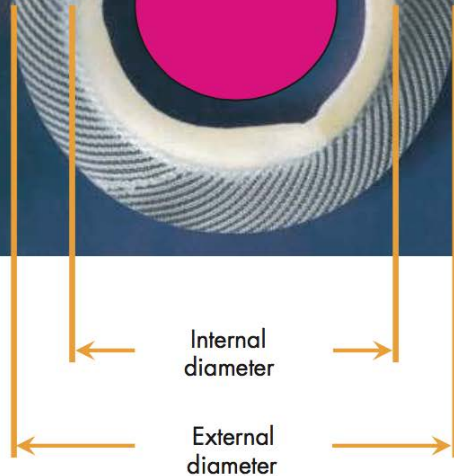
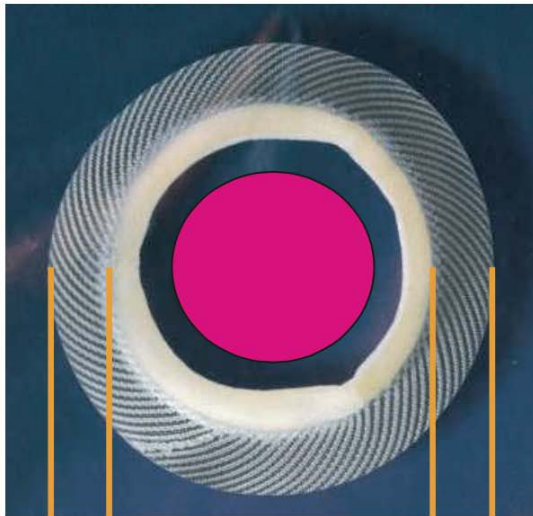
heart rate of the cardiac cycles used for Doppler measurements is particularly **important in mitral and tricuspid prosthetic valves**, because **the mean gradient is dependent on the diastolic filling period.**

Valve Size is not equal to EOA



EOA

Bioprosthetic valve



Mechanical valve

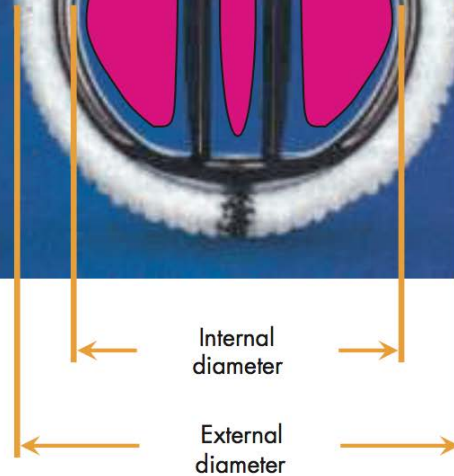
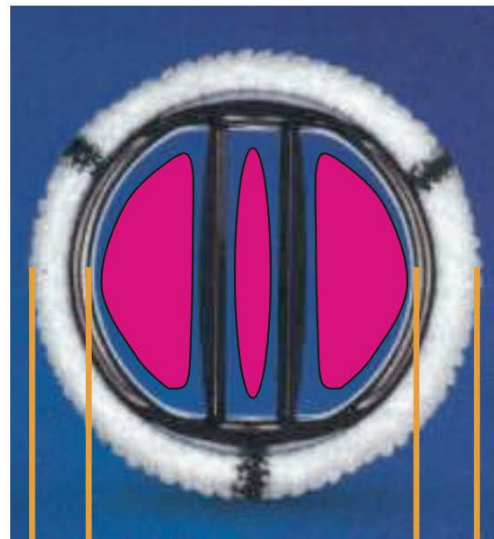


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	Presence of calcification on the leaflets or abnormal echo densities on the various components of the prosthesis
	Valve sewing ring integrity and motion
	Contour of the jet velocity
	Peak velocity and gradient
	Mean pressure gradient
	VTI of the jet
	DVI
	Pressure half-time in MV and TV
	EOA*
	Presence, location, and severity of regurgitation [†]
	LV and RV size, function, and hypertrophy
	LA and right atrial size
	Concomitant valvular disease
	Estimation of pulmonary artery pressure
	Comparison of above parameters is particularly helpful in suspected prosthetic valvular dysfunction

Thrombus?
Pannus?
Vegetation ?

Imaging of the valve

Opening and closing motion of the occluder

Doppler echocardiography of the valve

Effect on chambers

Compare with previous

Ro

c data

Previous postoperative studies, when available

Doppler Echocardiography

▣ Pressure Gradient

- ▣ Simplified Bernoulli equation: $4V^2$

▣ Effective Orifice Area

- ▣ Continuity equation: $EOA = \text{stroke volume} / VTI_{PrV}$
- ▣ Better index of valve function than gradient alone

- ▣ Dimensionless Index (DVI) = ratio of velocity proximal to the valve, to the velocity through the valve

Doppler Echocardiography

▣ Pressure Gradient

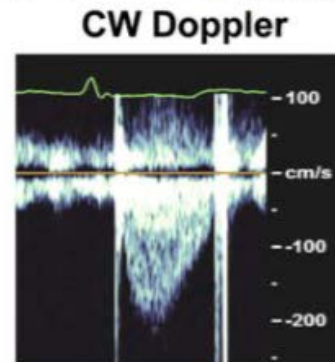
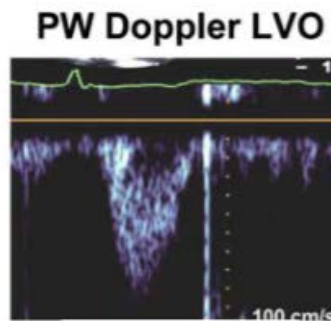
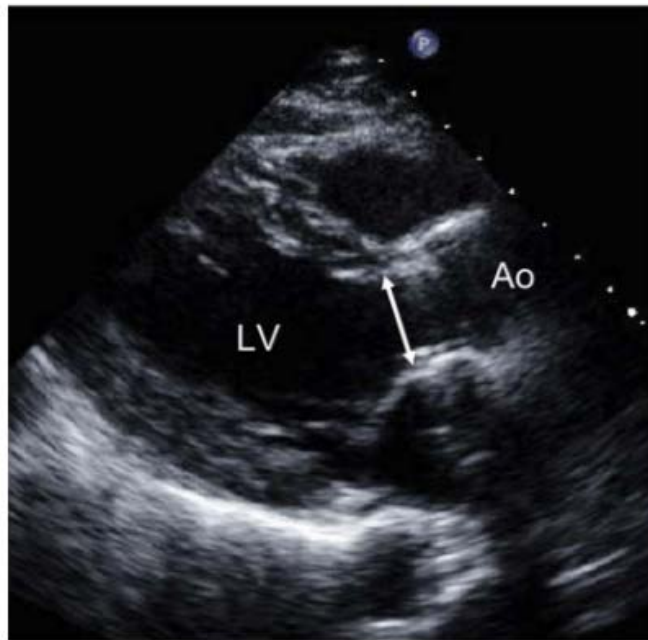
- ▣ Simplified Bernoulli equation: $4V^2$

▣ Effective Orifice Area

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Effective Orifice Area

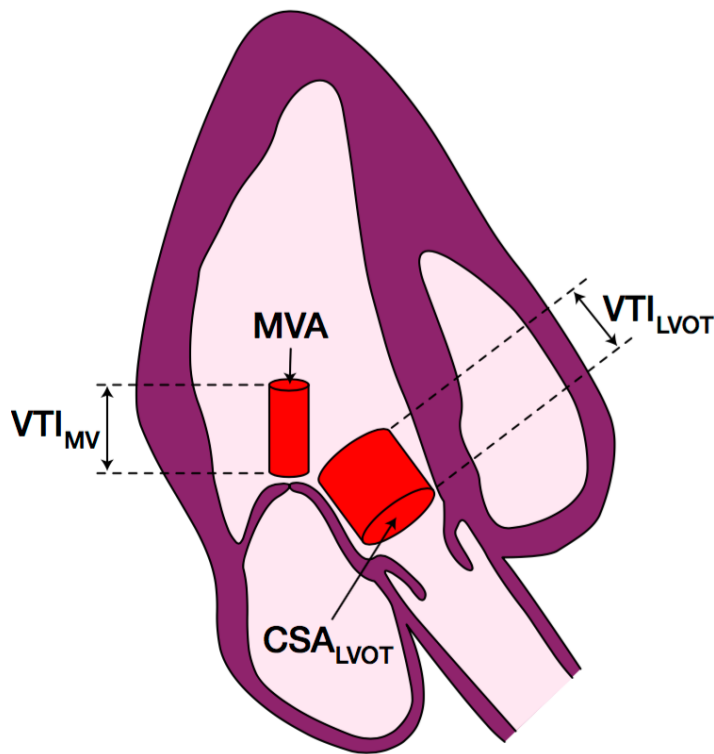


$$\text{Effective Orifice Area} = \frac{\text{CSA}_{\text{LVO}} \times \text{VTI}_{\text{LVO}}}{\text{VTI}_{\text{JET}}}$$

Pressure Half Time

- **not appropriate** to use the pressure half-time formula ($220/\text{pressure half-time}$) to estimate orifice area in prosthetic valves.
- valid only for **moderate or severe stenoses** ($< 1.5 \text{ cm}^2$).
- For larger valve areas, PHT reflects atrial and LV compliance characteristics and loading conditions and has no relation to valve area.

Mitral Valve Continuity Equation



(Equation 12.8)

$$MVA = \frac{CSA_{LVOT} \times VTI_{LVOT}}{VTI_{MV}}$$

where MVA = mitral valve area (cm²)

CSA_{LVOT} = cross-sectional area of left ventricular outflow tract (cm²)

VTI_{LVOT} = velocity time integral through the left ventricular outflow tract (cm)

VTI_{MV} = velocity time integral across the mitral valve (cm)

Doppler Echocardiography

- ▣ Pressure Gradient

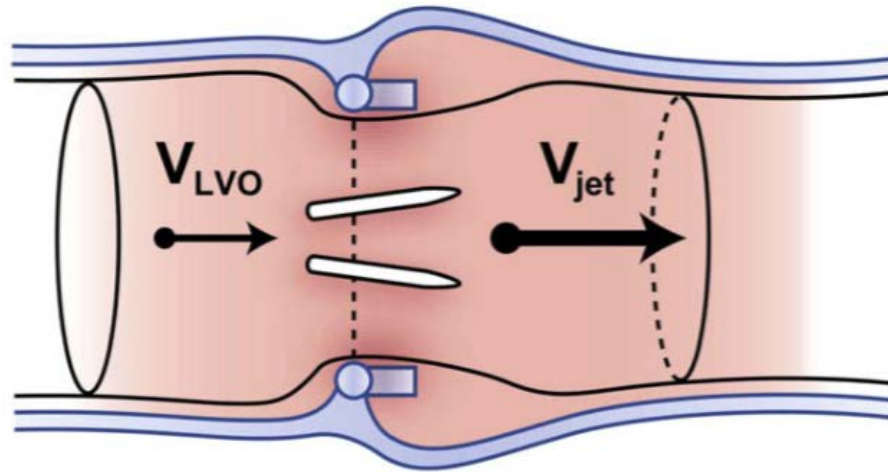
- ▣ Simplified Bernoulli equation: $4V^2$

- ▣ Effective Orifice Area

- ▣ Continuity equation: $EOA = \text{stroke volume} / VTI_{PrV}$
- ▣ Better index of valve function than gradient alone

- ▣ **Dimensionless Index (DVI)** = ratio of velocity proximal to the valve, to the velocity through the valve

Dimensionless Valve Index (DVI)



$$\text{Doppler Velocity Index} = \frac{\text{Velocity}_{LVO}}{\text{Velocity}_{jet}}$$

Figure 9 Schematic representation of the concept of the DVI. Velocity across the prosthesis is accelerated through the jet from the LVO tract. DVI is the ratio velocity in the LVO (V_{LVO}) to that of the jet (V_{jet}).

Early and Late Complications of Prosthetic Valves

PPM

Geometric mismatch

Dehiscence

Primary failure

Thrombosis and thromboembolism

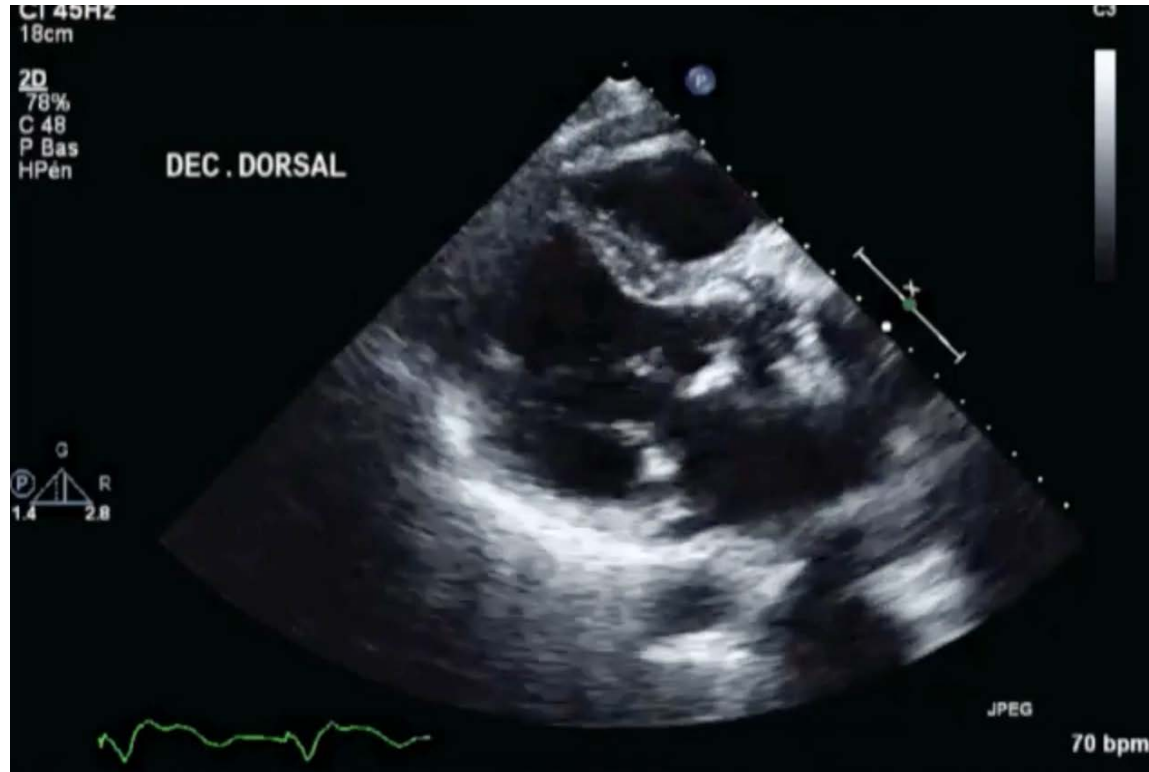
Pannus formation

Pseudoaneurysm formation

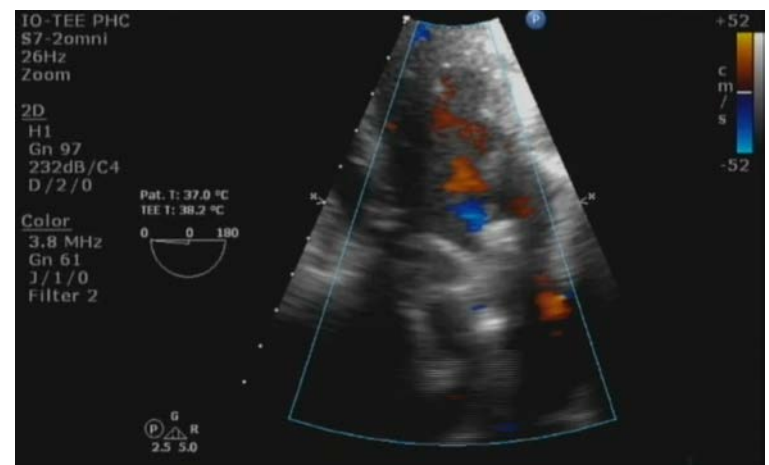
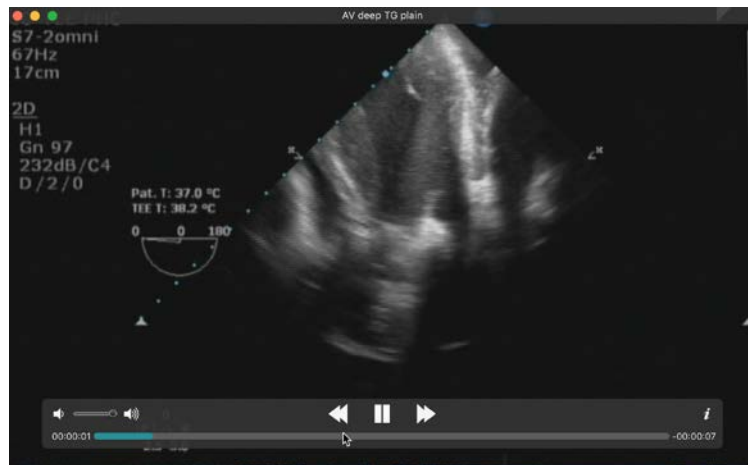
Endocarditis

Hemolysis

Normal Mechanical Prosthesis at Aortic Position



Normal Bi-leaflet Mechanical Aortic Valve (TEE)



Stented Bioprosthetic Mitral Valve



Prosthetic Valve Obstruction

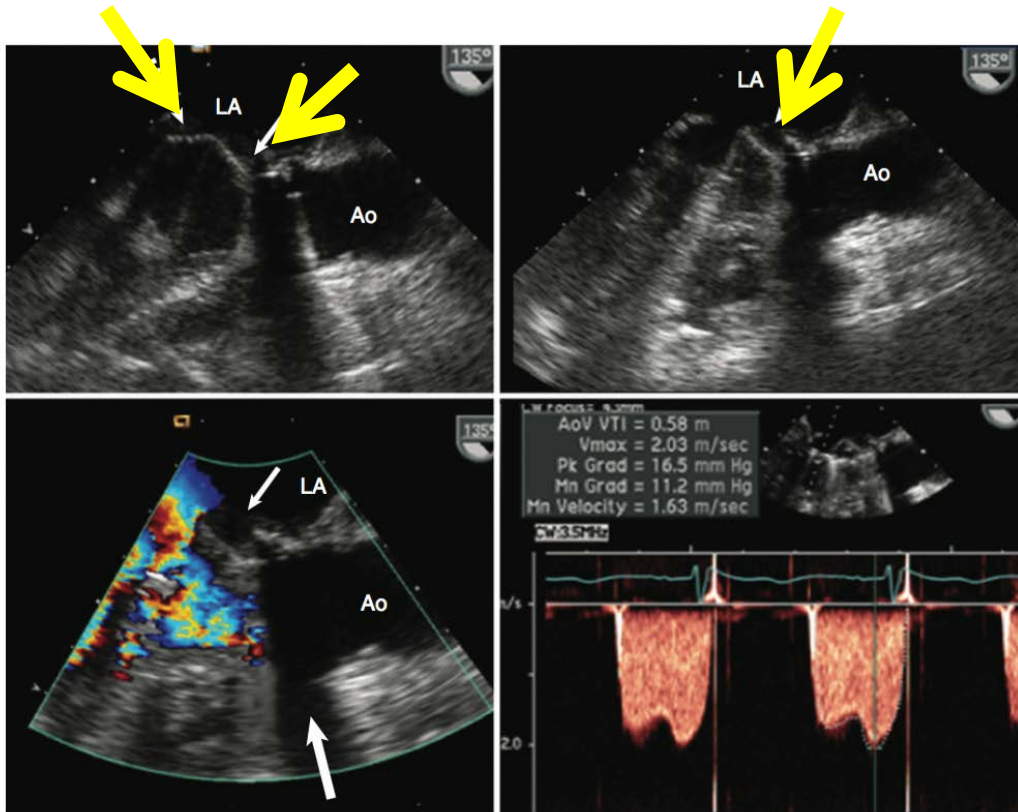
- ▣ Mechanical Valves: Thrombus or Pannus
- ▣ Bioprosthetic: structural valve degeneration (SVD)
 - ▣ (Abnormal leaflet morphology / mobility)
 - ▣ Increased gradient for valve subtype and size
 - ▣ Decreased EOA and DVI
 - ▣ Significant deviation from baseline study

#Importance of “finger printing” **iEOA and DVI typically unchanged** compared to baseline

Prosthetic Valve Obstruction: Thrombus

Systole:

both leaflets
doesn't
close fully



Diastole:

left disc
opens fully,
right disc
immobilized

High velocity
flow through
single orifice

Elevated
transmitral
gradient =
11.2 mmHg

Abnormal Mechanical Valve at Mitral Position

Decreased
occluder
motion and
thrombus at the
LV side of the
prosthesis



Pre- & post-thrombolysis of SJM mitral valve

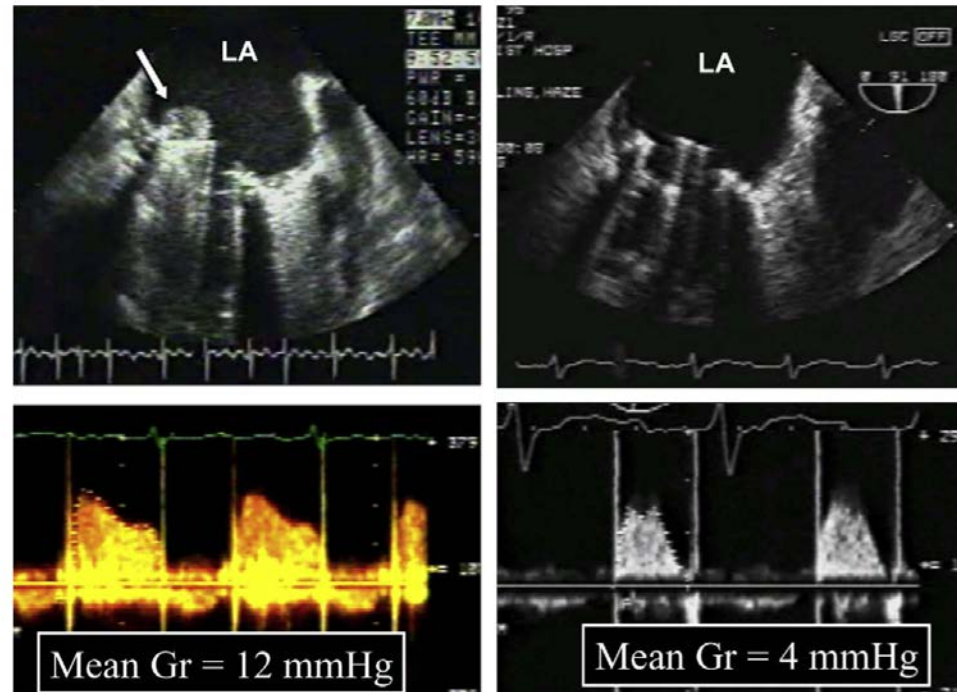
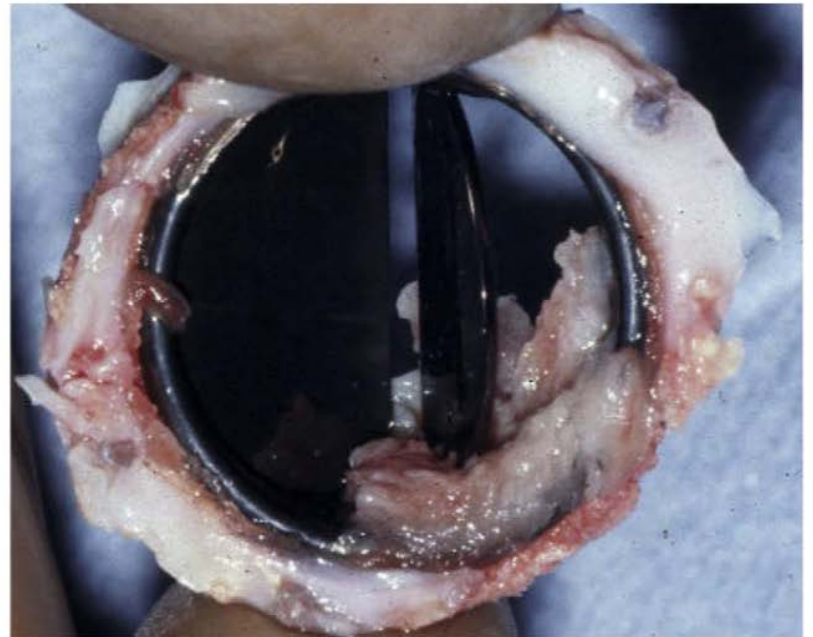
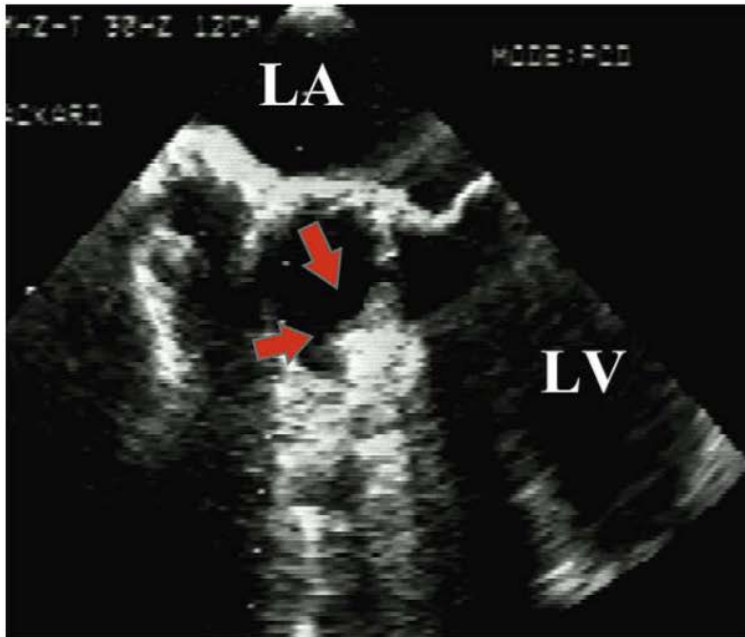
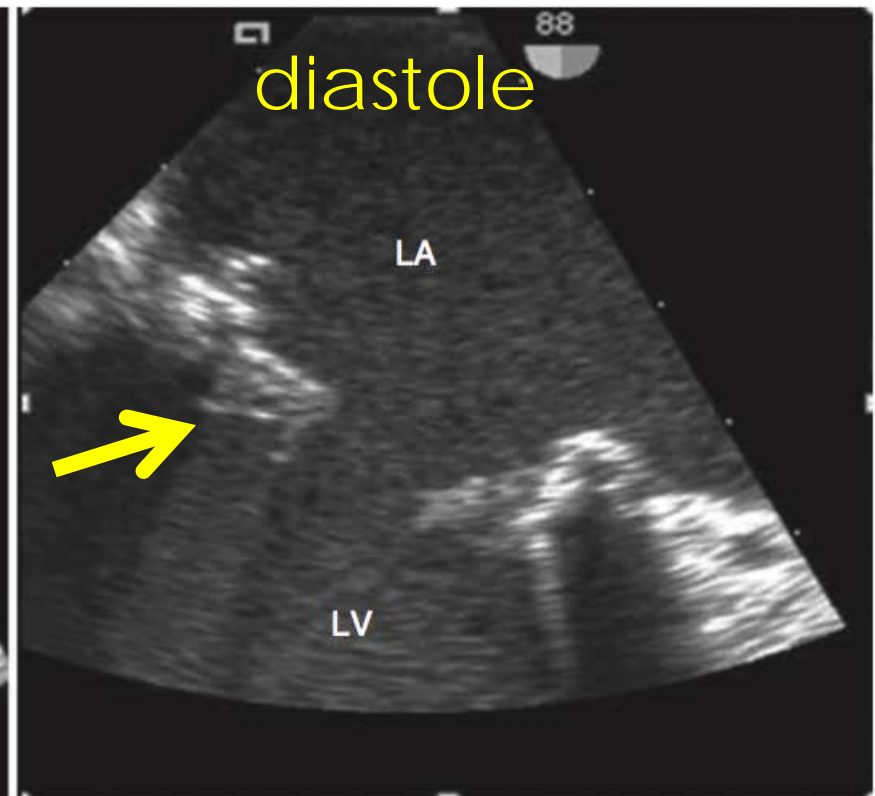
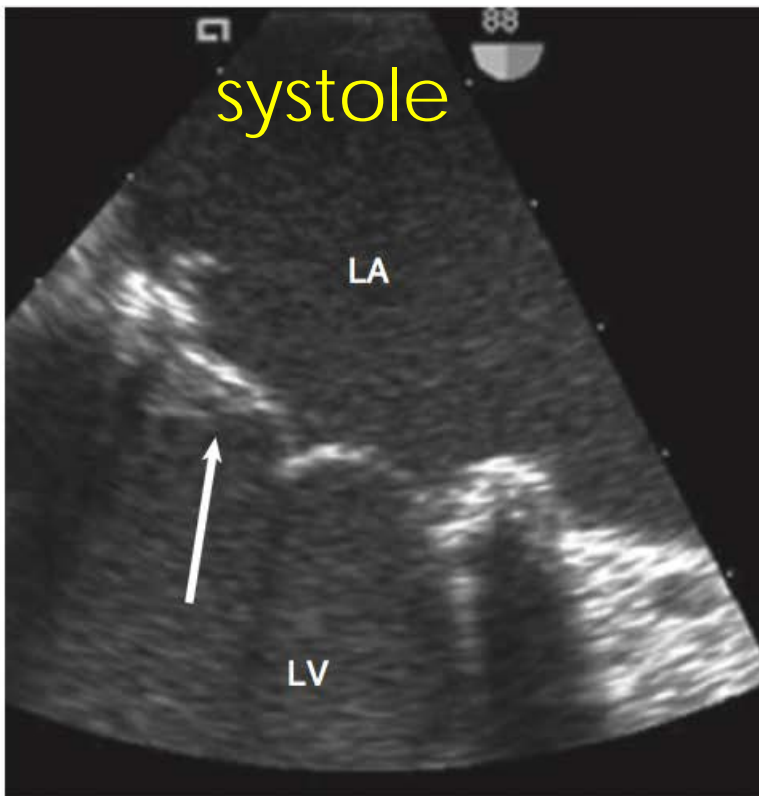


Figure 6 Prosthetic St Jude Medical valve thrombosis in the mitral position (arrow) obstructing and immobilizing one of the leaflets of the valve. After thrombolysis, leaflet mobility is restored, and the mean gradient (Gr) is significantly decreased. LA, Left atrium.

Pannus Formation in Mechanical Valve



Pannus Ingrowth Mitral Bioprosthesis



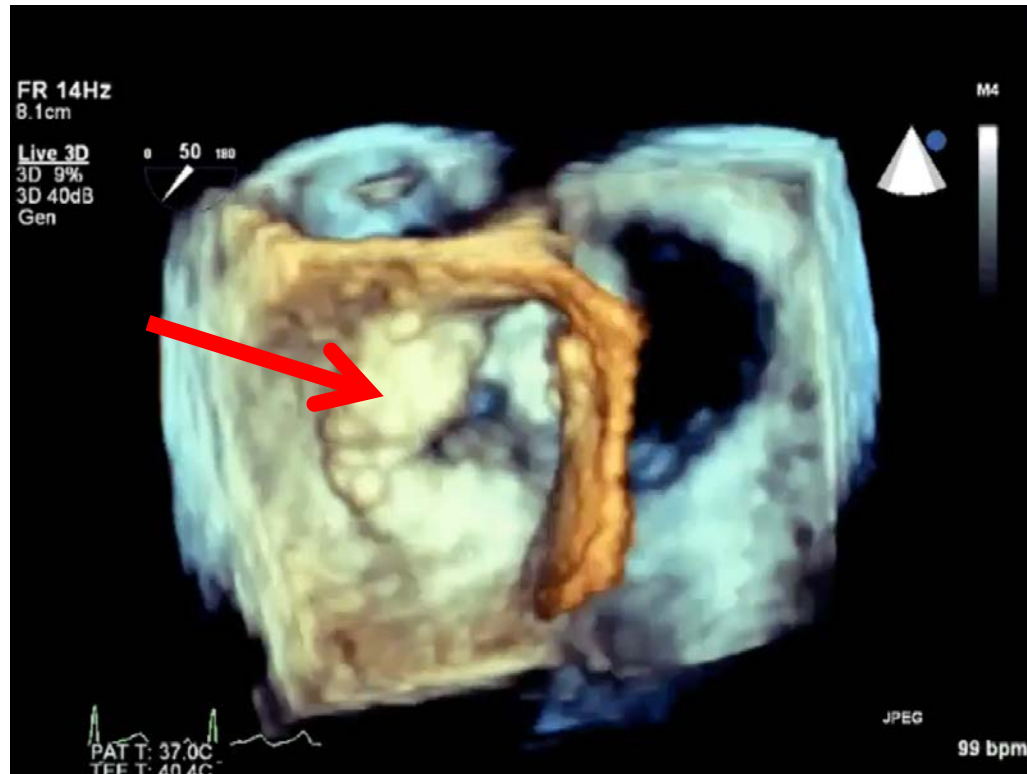
Pannus Bioprosthetic Valve

Elevated gradients across a bioprosthetic mitral valve

Pannus by TEE (echogenic area on the atrial side of the prosthesis)



Pannus formation



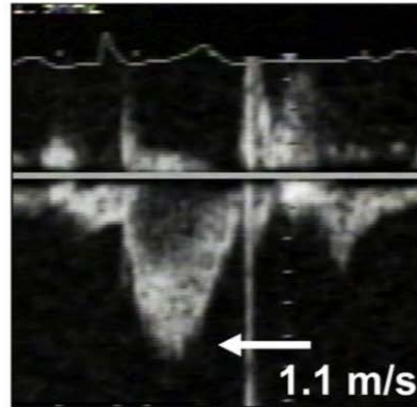
Evaluation of Prosthetic Valves by Location

Table 4 Doppler echocardiographic evaluation of prosthetic aortic valves

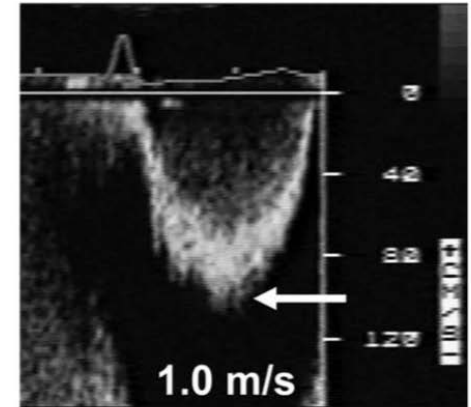
	Parameter
Doppler echocardiography of the valve	Peak velocity/gradient Mean gradient Contour of the jet velocity; AT DVI EOA Presence, location, and severity of regurgitation
Pertinent cardiac chambers	LV size, function, and hypertrophy

**Pulsed Doppler
LVO**

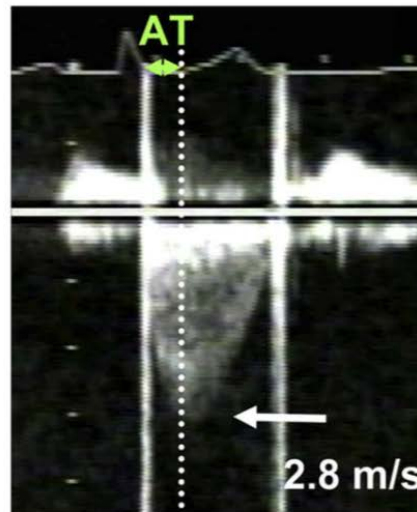
Normal



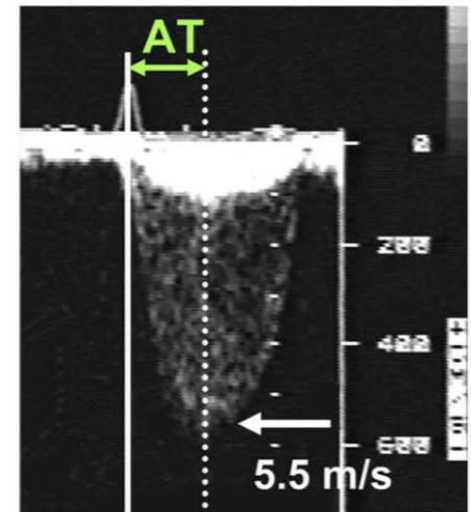
Obstructed



**CW Doppler
Prosthetic AV**



**MG = 22 mmHg
DVI = 0.4
AT = 75 ms**



**MG = 80 mmHg
DVI = 0.18
AT = 180 ms**

Doppler parameters of p

Obstructed

enosis

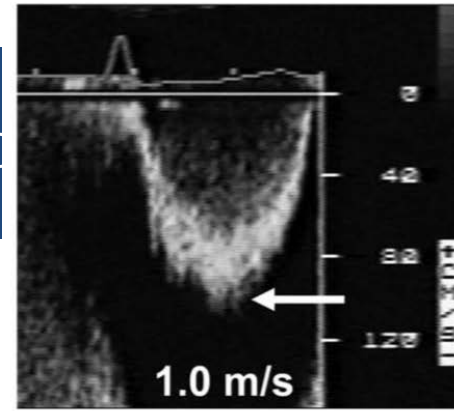


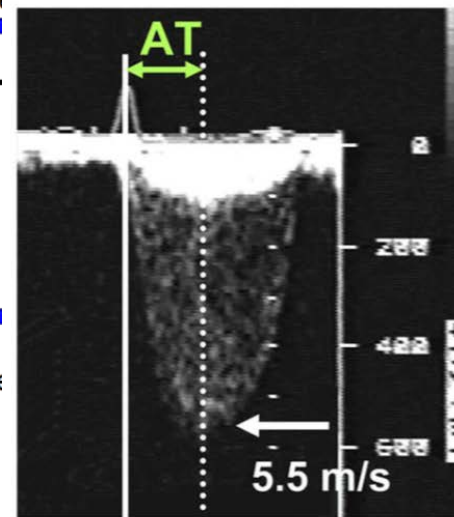
Table 5 Doppler parameters of prosthetic aortic valve function in m

Parameter	Normal
Peak velocity (m/s) [†]	<3
Mean gradient (mm Hg) [†]	<20
DVI	≥0.30
EOA (cm ²)	>1.2
Contour of the jet velocity through the PrAV	Triangular, early peaking
AT (ms)	<80

PrAV, Prosthetic aortic valve.

*In conditions of normal or near normal stroke volume (50-70 mL) through the

†These parameters are more affected by flow, including concomitant AR.



MG = 80 mmHg

DVI = 0.18

AT = 180 ms

ves*

Suggests significant stenosis
>4
>35
<0.25
<0.8
Rounded, symmetrical contour
>100

Inday – 41 year old female

Ht 149 cm Wt 53 kg **BSA 1.46 m²**

Concentric LVH LVMI = 119 gm/2,
RWT = 0.53, LVEF 74%

Aortic root = 2.8 cm

LVOT dia = 2.1 cm

LVOT VTI = 26.7

Ao VTI = 98.1

DVI = 0.27

EOA = 0.94 cm²

iEOA = 0.64

MVG = 42 mmHg

PIG = 89 mmg

SPAP = 33 mmHg



Prosthesis Patient Mismatch

- No detectable structural abnormality of the PV leaflets / occluders
- Normal EOA and DVI for subtype
- $iEOA \leq 0.85$ **(0.64)**

Consequences of PPM

- ❑ Worse hemodynamics
- ❑ Less regression of LVH (and pulmonary HPN)
- ❑ Worse functional class, exercise capacity, and quality of life
- ❑ More cardiac events
- ❑ Lower survival

Indexed EOA is the only parameter shown to have any correlation with post-operative gradients &/or outcomes in **prosthetic valve mismatch**

Determinants of Mismatch

- ▣ larger BSA - **higher cardiac output requirements**
- ▣ older age
- ▣ smaller prosthesis size (\leq size19)
- ▣ valvular stenosis as the predominant lesion before the operation



Prevention of PPM

STEP 1:
 Calculate BSA = **1.64**

Table 1. Three Easy Steps to Avoid Prosthesis–Patient Mismatch

Step I: Calculate the patient’s body surface (BSA) area using the formula:

$$BSA = ([Weight_{kg}]^{0.425} \times [height_{cm}]^{0.725}) \times 0.007184$$

Step II: Determine the minimal requirement for prosthetic valve effective orifice area (EOA) to avoid prosthesis–patient mismatch.

STEP 2:
 Determine minimal projected EOA

BSA x 0.85
 1.64 x 0.85 =
1.394

Patient BSA (m ²)	Minimal Valve EOA (cm ²) for Indexed EOA >0.85 cm ² /m ² (Ideal)	Minimal Valve EOA (cm ²) for Indexed EOA >0.80 cm ² /m ²	Minimal Valve EOA (cm ²) for Indexed EOA >0.75 cm ² /m ²
1.30	1.11	1.04	0.98
1.35	1.15	1.08	1.01
1.40	1.20	1.12	1.05
1.45	1.23	1.16	1.09
1.50	1.28	1.20	1.13
1.55	1.32	1.24	1.16
1.60	1.36	1.28	1.20
1.65	1.40	1.32	1.24
1.70	1.45	1.36	1.28
1.75	1.49	1.40	1.31
1.80	1.53	1.44	1.35
1.85	1.57	1.48	1.39
1.90	1.62	1.52	1.43
1.95	1.66	1.56	1.46
2.00	1.70	1.60	1.50
2.05	1.74	1.64	1.54
2.10	1.79	1.68	1.58
2.15	1.83	1.72	1.61
2.20	1.87	1.76	1.65
2.25	1.91	1.80	1.69
2.30	1.96	1.84	1.73
2.35	2.00	1.88	1.76
2.40	2.04	1.92	1.80
2.45	2.08	1.96	1.84
2.50	2.13	2.00	1.88

STEP 3:
 Choose prosthesis using reference values for EOA

Step III: Choose a prosthesis using reference values for EOA of different types and sizes of prostheses (see Table 2).

	EOAi by Prosthesis size (mm)					
Prosthesis size (mm)	19	21	23	25	27	29
Average EOA (cm ²)	1.1	1.3	1.5	1.8	2.3	2.7
BSA (m²)						
0.6	1.83	2.17	2.50	3.00	3.83	4.50
0.7	1.57	1.86	2.14	2.57	3.29	3.86
0.8	1.38	1.63	1.88	2.25	2.88	3.38
0.9	1.22	1.44	1.67	2.00	2.56	3.00
1	1.10	1.30	1.50	1.80	2.30	2.70
1.1	1.00	1.18	1.36	1.64	2.09	2.45
1.2	0.92	1.08	1.25	1.50	1.92	2.25
1.3	0.85	1.00	1.15	1.38	1.77	2.08
1.4	0.79	0.93	1.07	1.29	1.64	1.93
1.5	0.73	0.87	1.00	1.20	1.53	1.80
1.6	0.49	0.88	0.88	0.88	0.88	1.69
1.7	0.65	0.76	0.88	1.06	1.35	1.59
1.8	0.61	0.72	0.83	1.00	1.28	1.50
1.9	0.58	0.68	0.79	0.95	1.21	1.42
2	0.55	0.65	0.75	0.90	1.15	1.35
2.1	0.52	0.62	0.71	0.86	1.10	1.29
2.2	0.50	0.59	0.68	0.82	1.05	1.23
2.3	0.48	0.57	0.65	0.78	1.00	1.17
2.4	0.46	0.54	0.63	0.75	0.96	1.13
2.5	0.44	0.52	0.60	0.72	0.92	1.08

STEP 3:

Choose prosthesis using reference values for EOA

1.4

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Prosthesis-Patient Mismatch

Table 2. Normal Effective Orifice Areas for the Most Currently Used Prosthetic Valves

Prosthetic Valve Size (mm)	19	21	23	25	27	29	Reference no.
Stented Bioprosthetic valves							
Medtronic Intact	0.85	1.02 ± 0.10	1.27 ± 0.11	1.40 ± 0.20	1.66 ± 0.16	2.04 ± 0.23	(2)
Medtronic Mosaic	—	1.22 ± 0.27	1.38 ± 0.23	1.65 ± 0.39	1.59 ± 0.33	1.65 ± 0.37	(95)
Hancock II	—	1.18 ± 0.11	1.33 ± 0.16	1.46 ± 0.15	1.55 ± 0.18	1.60 ± 0.15	(3)
Carpentier-Edwards SAV 2650	—	1.16 ± 0.14	—	—	—	—	(96)
Carpentier-Edwards Pericardial 2900	1.10	1.30	1.50	1.80	1.60	—	(97)
Stentless bioprosthetic valves							
Medtronic Freestyle	1.15	1.35 ± 0.21	1.48 ± 0.33	2.00 ± 0.39	2.32 ± 0.48	—	(39)
	1.29 ± 0.19	<u>1.46 ± 0.32</u>	1.79 ± 0.33	2.34 ± 0.69	2.67 ± 0.75	—	(98)
St. Jude Medical Toronto SPV	—	1.30	1.50	1.70	2.00	2.50	(SJM†)
	—	—	<u>1.49 ± 0.45</u>	1.70 ± 0.78	2.12 ± 0.66	2.70 ± 1.03	(99)
Prima Edwards	0.80	1.10	<u>1.50</u>	1.80	2.30	2.80	(100)
Mechanical valves							
Medtronic Hall	1.19 ± 0.21*	1.34 ± 0.15	—	—	—	—	(96)
Carbomedics Standard	1.00 ± 0.40	<u>1.54 ± 0.31</u>	1.63 ± 0.30	1.98 ± 0.41	2.41 ± 0.46	2.63 ± 0.38	(93)
	1.11 ± 0.13	<u>1.52 ± 0.22</u>	1.84 ± 0.25	2.12 ± 0.31	2.65 ± 0.21	—	(14)
St. Jude Medical Standard	—	1.73 ± 0.38	2.13 ± 0.61	—	—	—	(101)
	—	1.76 ± 0.47	2.11 ± 0.63	—	—	—	(26)
	1.04 ± 0.19	1.38 ± 0.22	1.52 ± 0.26	2.08 ± 0.41	2.65 ± 0.58	3.23 ± 0.30	(13)
St. Jude Medical Hemodynamic Plus	1.30 ± 0.30	—	—	—	—	—	(102)
	—	2.01 ± 0.17	—	—	—	—	(101)
	—	2.15 ± 0.29	—	—	—	—	(26)

*The label valve size of this valve is 20 mm. †Data provided by St. Jude Medical.

Effective orifice areas are expressed as the mean value ±SD cm². The effective orifice areas were measured by Doppler echocardiography using the continuity equation in patients with normally functioning prostheses. Some data appear conflicting or are based on limited series and may have to be revised as more data become available.

Evaluation of Prosthetic Valve by Location

Table 7 Echocardiographic and Doppler parameters in evaluation of prosthetic mitral valve function (stenosis or regurgitation)

Doppler echocardiography of the valve	Peak early velocity Mean gradient Heart rate at the time of Doppler Pressure half-time DVI*: VTI_{PrMV}/VTI_{LVO} EOA* Presence, location, and severity of regurgitation [†]
Other pertinent echocardiographic and Doppler parameters	LV size and function LA size [‡] RV size and function Estimation of pulmonary artery pressure

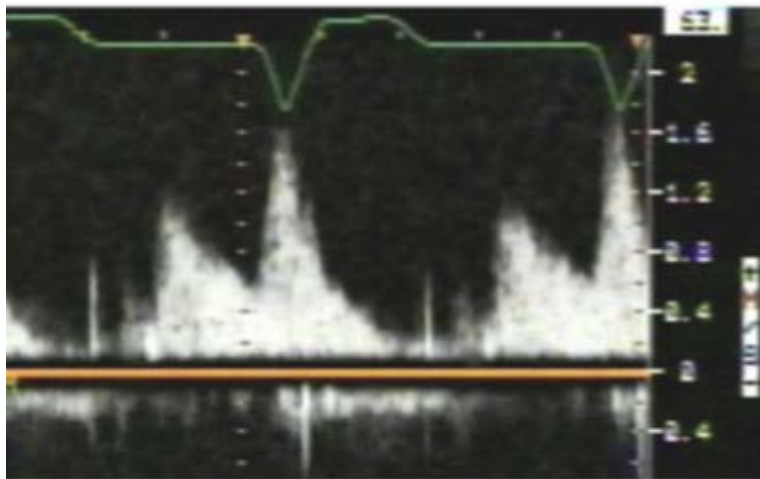
Doppler Evaluation of Mitral Stenosis

Table 8 Doppler parameters of prosthetic mitral valve function

	Normal*	Possible stenosis [‡]	Suggests significant stenosis* [‡]
Peak velocity (m/s) ^{† §}	<1.9	1.9-2.5	≥2.5
Mean gradient (mm Hg) ^{† §}	≤5	6-10	>10
VTI _{PrMv} /VTI _{LVO} ^{† §}	<2.2	2.2-2.5	>2.5
EOA (cm ²)	≥2.0	1-2	<1
PHT (ms)	<130	130-200	>200

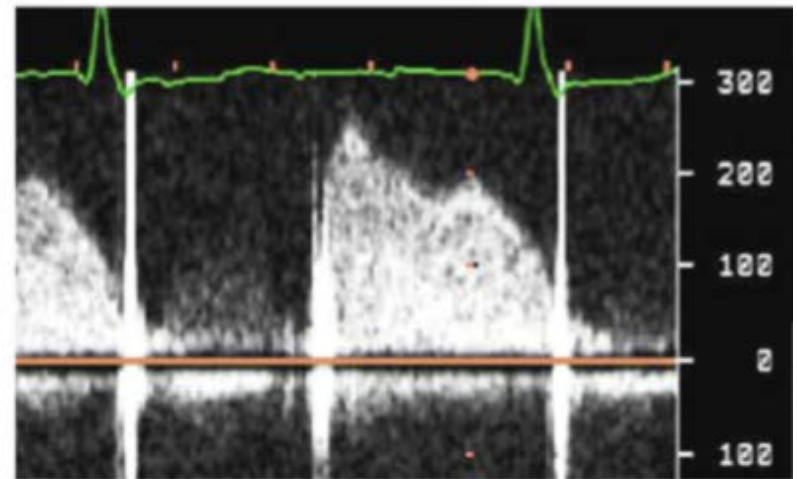
Doppler Evaluation of Mitral Prosthesis

Normal



Peak E = 1.1 m/s
Mean G = 4 mmHg
PHT = 123 ms

Obstructed



Peak E = 2.5 m/s
Mean G = 15 mmHg
PHT = 170 ms

Degenerated Mitral Bioprosthesis



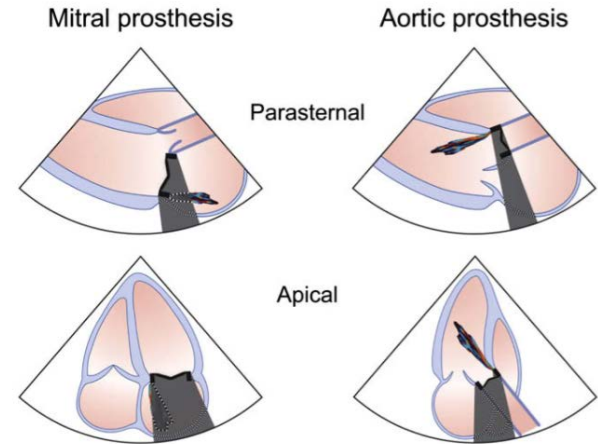
Physiologic vs Pathologic Regurgitation

- ▣ **Washing jets** to prevent thrombus formation
- ▣ 10-15%
- ▣ Jets low in momentum
 - ▣ homogeneous in color,
 - ▣ aliasing mostly confined to the base of the jet.

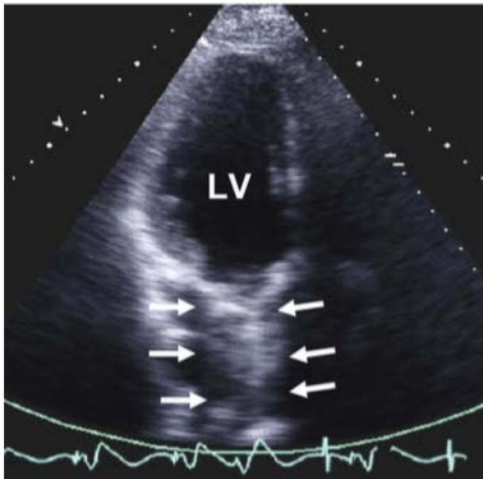
- ▣ **Central**

- ▣ **Paravalvular**

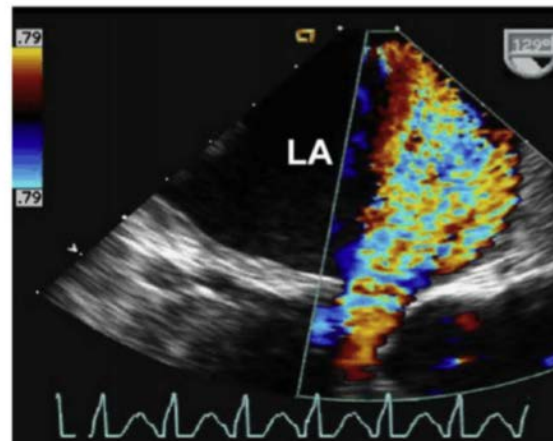
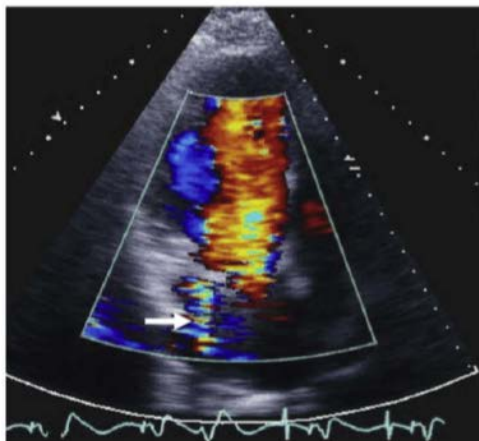
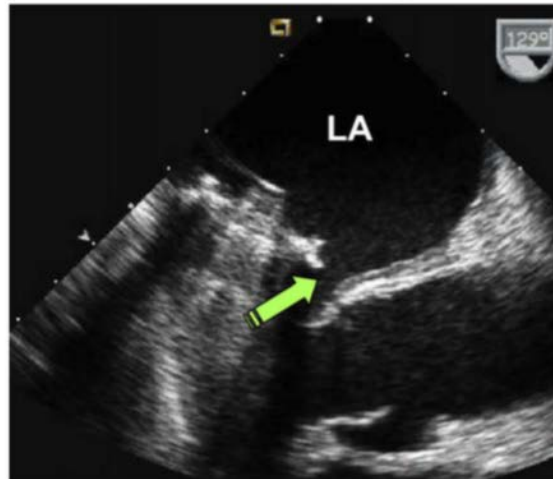
Severe Paravalvular MR



Transthoracic



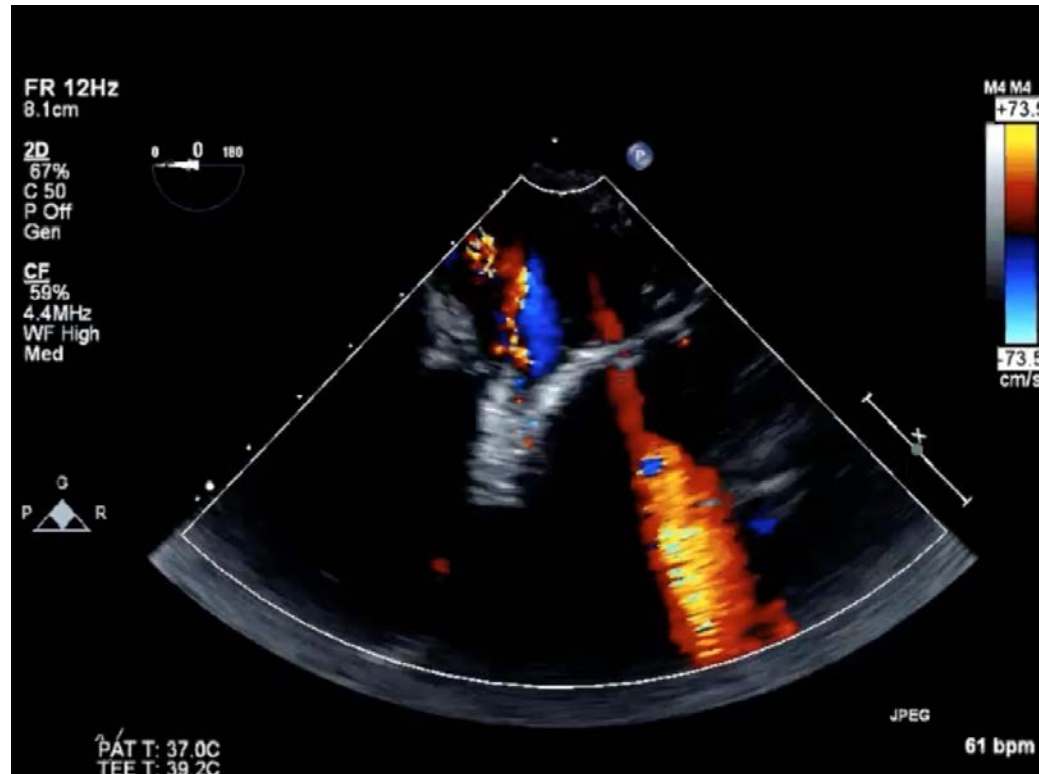
Transesophageal



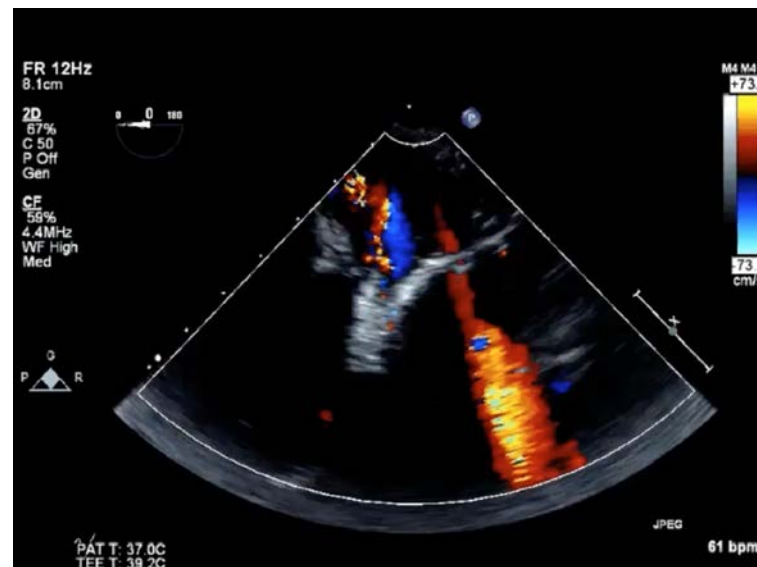
Mild central MR across a bioprosthesis



Large paravalvular leak



Dehiscence

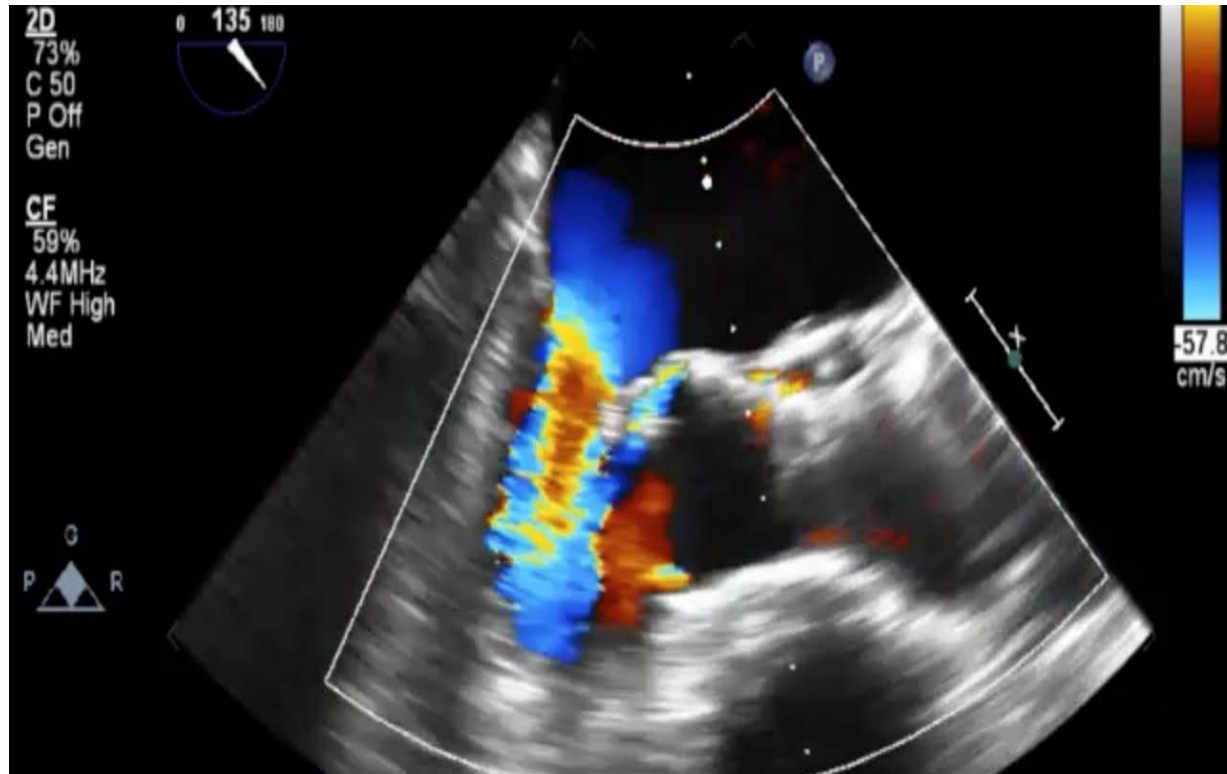


Paravalvular Leak





Periprosthetic Leak (CoreValve)



Significant Mechanical Mitral Regurgitation

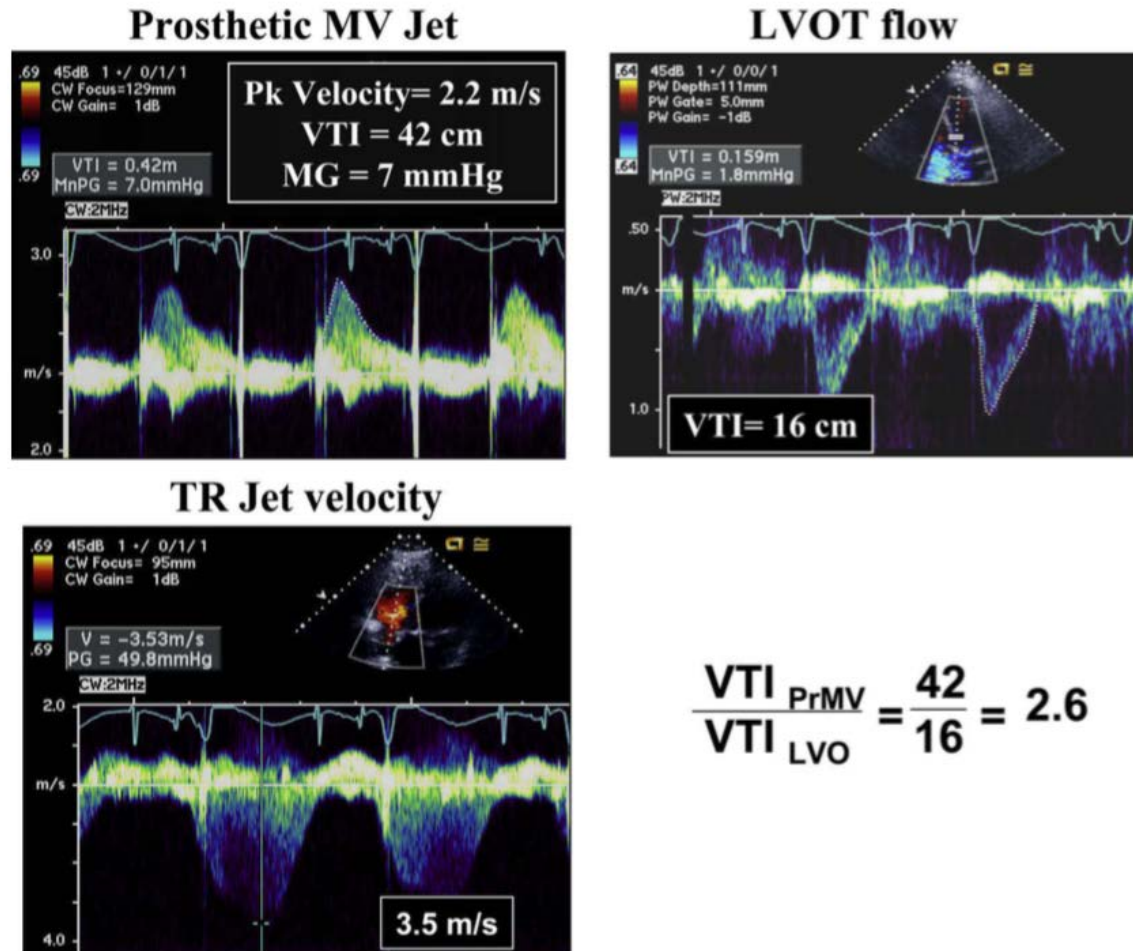


Figure 13 Transthoracic Doppler echocardiographic clues for significant mechanical MR. These recordings are for the same patient

Table 9 Transthoracic echocardiographic findings suggestive of significant prosthetic MR in mechanical valves with normal pressure half-time

Finding	Sensitivity	Specificity	Comments
Peak mitral velocity ≥ 1.9 m/s*	90%	89%	Also consider high flow, PPM
$VTI_{PrMV}/VTI_{LVO} \geq 2.5^*$	89%	91%	Measurement errors increase in atrial fibrillation due to difficulty in matching cardiac cycles; also consider PPM
Mean gradient ≥ 5 mmHg*	90%	70%	At physiologic heart rates; also consider high flow, PPM
Maximal TR jet velocity > 3 m/s*	80%	71%	Consider residual postoperative pulmonary hypertension or other causes
LV stroke volume derived by 2D or 3D imaging is $>30\%$ higher than systemic stroke volume by Doppler	Moderate sensitivity	Specific	Validation lacking; significant MR is suspected when LV function is normal or hyperdynamic and VTI_{LVO} is <16 cm
Systolic flow convergence seen in the left ventricle toward the prosthesis	Low sensitivity	Specific	Validation lacking; technically challenging to detect readily

Severity of Prosthetic Aortic Valve Regurgitation

Table 6 Parameters for evaluation of the severity of prosthetic aortic valve regurgitation

Parameter	Mild	Moderate	Severe
Valve structure and motion			
Mechanical or bioprosthetic	Usually normal	Abnormal [†]	Abnormal [†]
Structural parameters			
LV size	Normal [‡]	Normal or mildly dilated [‡]	Dilated [‡]
Doppler parameters (qualitative or semiquantitative)			
Jet width in central jets (% LVO diameter): color*	Narrow ($\leq 25\%$)	Intermediate (26%-64%)	Large ($\geq 65\%$)
Jet density: CW Doppler	Incomplete or faint	Dense	Dense
Jet deceleration rate (PHT, ms): CW Doppler [§]	Slow (>500)	Variable (200-500)	Steep (<200)
LVO flow vs pulmonary flow: PW Doppler	Slightly increased	Intermediate	Greatly increased
Diastolic flow reversal in the descending aorta: PW Doppler	Absent or brief early diastolic	Intermediate	Prominent, holodiastolic
Doppler parameters (quantitative)			
Regurgitant volume (mL/beat)	<30	30-59	>60
Regurgitant fraction (%)	<30	30-50	>50

PHT, Pressure half-time.

*Parameter applicable to central jets and is less accurate in eccentric jets; Nyquist limit of 50 to 60 cm/s.

[†]Abnormal mechanical valves, for example, immobile occluder (valvular regurgitation), dehiscence or rocking (paravalvular regurgitation); abnormal biologic valves, for example, leaflet thickening or prolapse (valvular), dehiscence or rocking (paravalvular regurgitation).

[‡]Applies to chronic, late postoperative AR in the absence of other etiologies.

[§]Influenced by LV compliance.

Severity of Mitral Regurgitation

Table 10 Echocardiographic and Doppler criteria for severity of prosthetic MR using findings from TTE and TEE

Parameter	Mild	Moderate	Severe
Structural parameters			
LV size	Normal*	Normal or dilated	Usually dilated [‡]
Prosthetic valve	Usually normal	Abnormal [¶]	Abnormal [¶]
Doppler parameters			
Color flow jet area [#]	Small, central jet (usually <4 cm ² or <20% of LA area)	Variable	Large central jet (usually >8 cm ² or >40% of LA area) or variable size wall-impinging jet swirling in left atrium
Flow convergence ^{**}	None or minimal	Intermediate	Large
Jet density: CW Doppler	Incomplete or faint	Dense	Dense
Jet contour: CW Doppler	Parabolic	Usually parabolic	Early peaking, triangular
Pulmonary venous flow	Systolic dominance [§]	Systolic blunting [§]	Systolic flow reversal [†]
Quantitative parameters^{††}			
VC width (cm)	<0.3	0.3-0.59	≥0.6
R vol (mL/beat)	<30	30-59	≥60
RF (%)	<30	30-49	≥50
EROA (cm ²)	<0.20	0.20-0.49	≥0.50

A close-up photograph of a hand in a dark suit sleeve giving a thumbs up gesture. The hand is the central focus, with the thumb pointing upwards. A semi-transparent black horizontal band is overlaid across the middle of the image, containing the text 'THANK YOU FOR YOUR ATTENTION' in white, bold, uppercase letters.

THANK YOU FOR YOUR ATTENTION